

### E.M processes implemented

#### • E.M. Standard

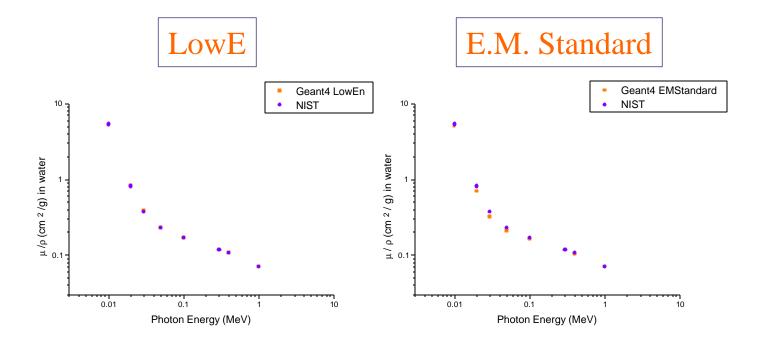
- •G4PhotoElectricEffect
- •G4ComptonScattering
- •G4GammaConversion

#### • Low Energy

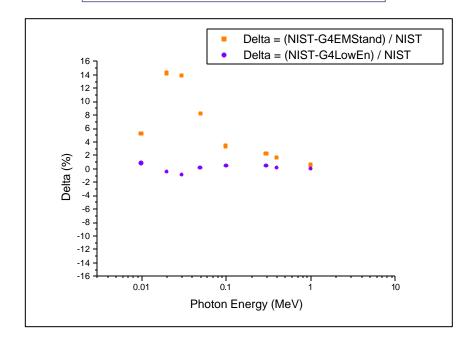
- •G4LowEnergyRayleigh
- •G4LowEnergyPhotoElectric
- •G4LowEnergyCompton
- •G4LowEnergyGammaConversion

Simulation in water, iron, lead with E.M.Standard and LowE extension and comparison with the National Institute for Standard and Technology (NIST) data

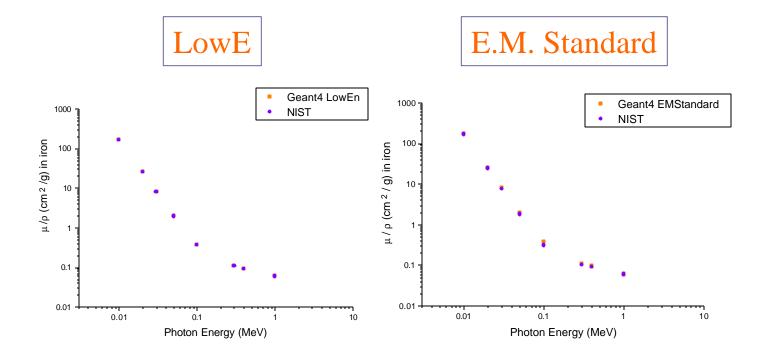
# Photon mass attenuation coefficient, Water

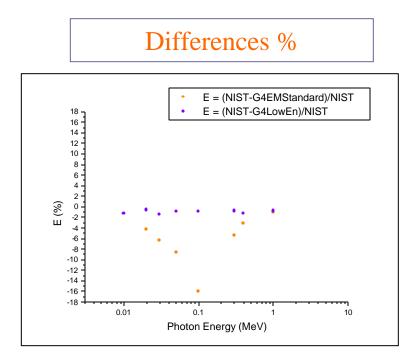


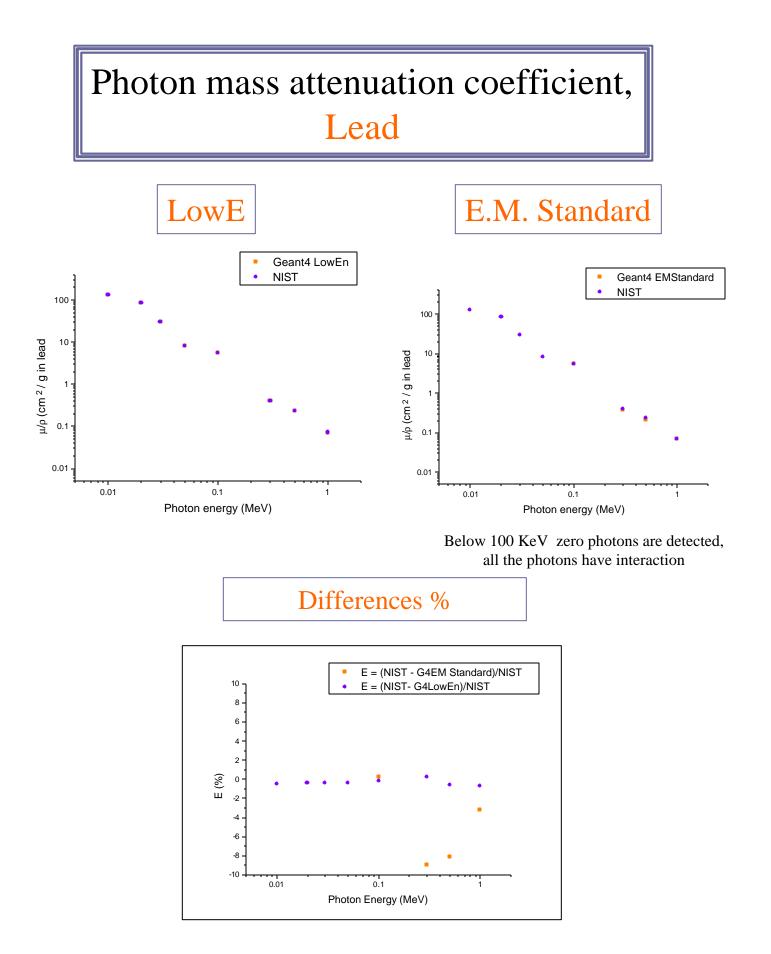
Differences %



# Photon mass attenuation coefficient, Iron

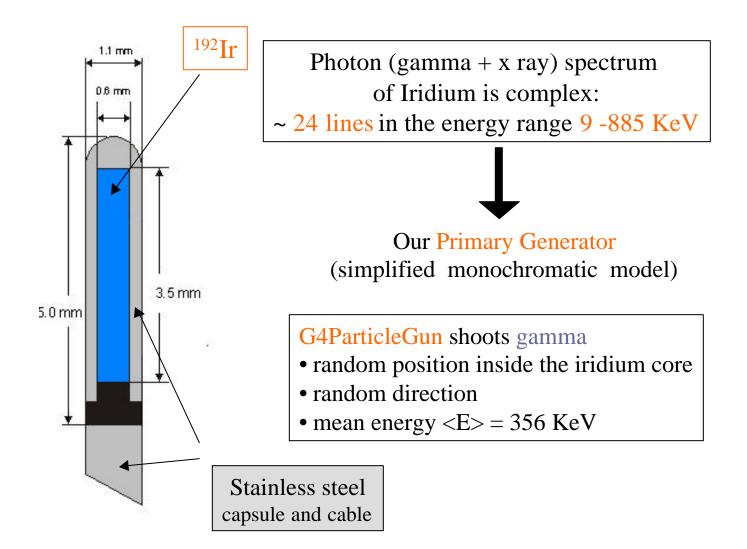






## Determination of the isodose distribution in water around a <sup>192</sup>Ir source

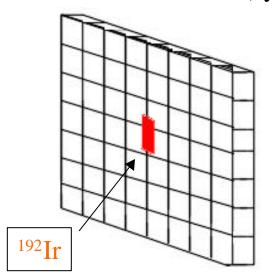




### Geometrical set-up

The source is placed inside a 30 cm water box which is associated with a Sensitive Detector object

> We wish to determine the energy deposition in water around the source in a longitudinal plane (cylindrical symmetry)



#### **Readout Geometry**

The longitudinal plane is portioned in 300 · 300, 1 mm<sup>3</sup>, voxels

At every interaction, energy deposition is scored and stored in the relevant voxel (in a matrix)

#### EM Processes implemented

• G4MultipleScattering

#### gamma

- G4LowEnergyRayleigh
- G4LowEnergyPhotoElectric
- G4LowEnergyCompton
- G4LowEnergyGammaConversion

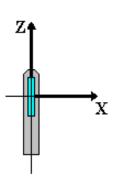
#### e-

- G4LowEnergyIonisation
- G4LowEnergyBremsstrahlung

#### e+

- G4eIonisation
- G4eBremsstrahlung
- G4eplusAnnihilation

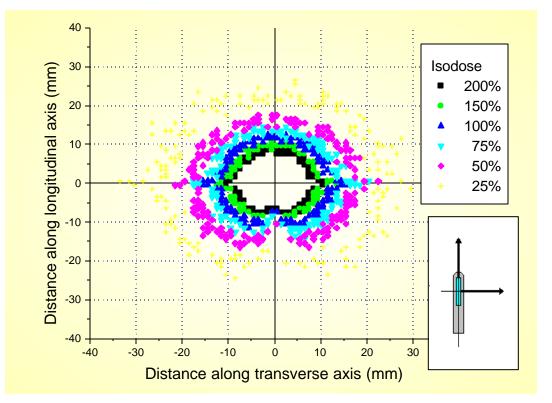
## Output



As in the advanced Brachytherapy example,

at the end of the RUN an ASCII file is produced for further processing with X,Z energy deposition Isodose distribution in water around a <sup>192</sup>Ir source

20 10 <sup>6</sup> photons generated
~ 24 hours of simulation

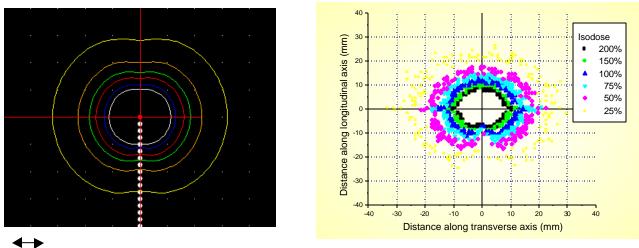


The dose deposition is not isotropic due to

- •source geometry
- •auto-absorption,
- •encapsulation and shielding effects

At the bottom centre of the source we can see the effect of the stainless steel cable

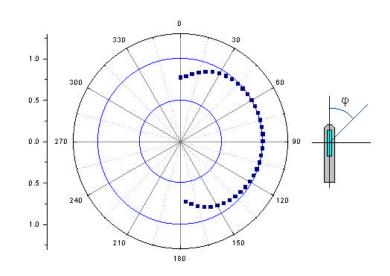
# Comparison with isodoses of the *Plato* treatment planning system

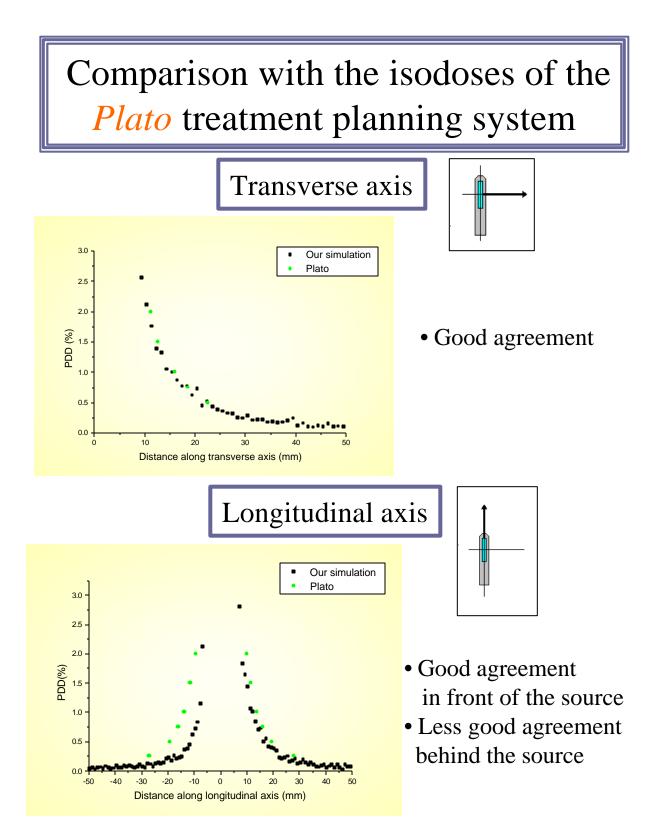


#### 1 cm

*Plato* uses an analytical method to calculate the dose distribution:

- Point approximation of the source to compute the dose
- Anisotropy function F(φ), instead of F(r,φ) as it should be, to account for the shielding effect of the capsule, etc..



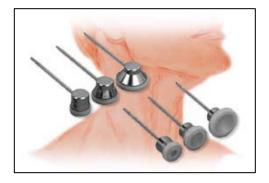


The disagreement in the region behind the source is due to the approximation introduced by the anisotropy function in this direction

Geant4 yields a more realistic behaviour

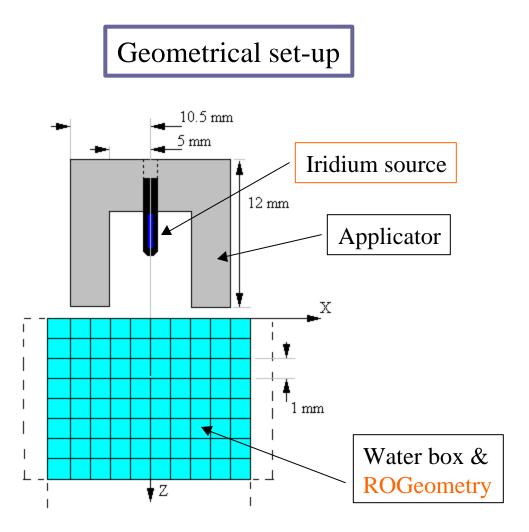
Initial results for the

Leipzig applicator

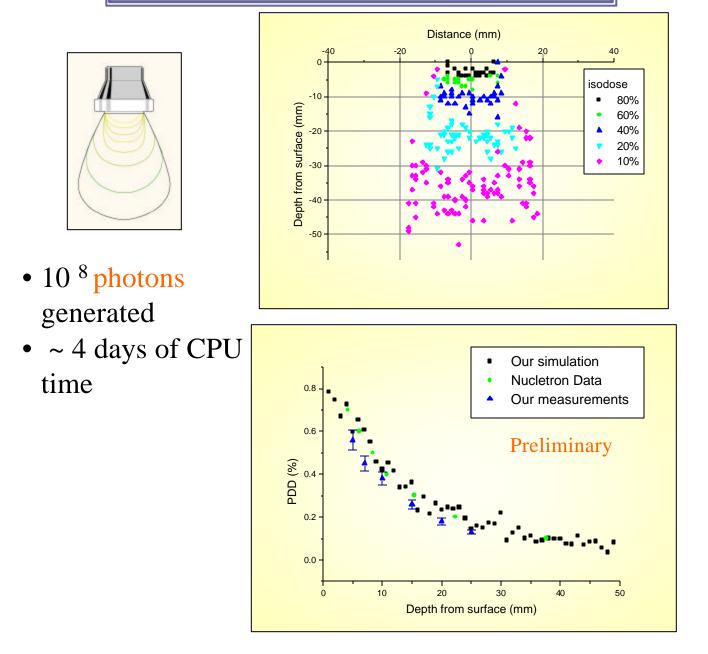


The Leipzig applicators were designed to give the optimum isodoses and treat to the correct depth

This applicator has the shape of a hollow cylinder of tungsten containing the source



# Isodose distribution in water for the Leipzig applicator



These are the initial results with this kind of applicator

- good agreement with manufacturer's data (Nucletron)
- satisfactory agreement with our measurements (we have just started making measurements and the systematic errors for the response of the detector are not well known yet)



Our activities at

- Porting on Windows 98+Cygwin+VisualC++ environment
- Simple test for the EM processes
- Application in the medical field Simulation for isodose distribution and comparison of the result with those of our TPS and measure
- Promotion of Geant4 with poster and oral presentation in several medical physics congress (AIFM, ESTRO, AIRO, ...)

We think that Geant4 is an useful instrument in medical radiation physics Its use out of the HEP community could be advantageous both for users (as we are) and for the code developers